

Computational approaches for understanding energy metabolism

Alexander A. Shestov,¹ Brandon Barker,^{1,2} Zhenglong Gu^{1,2} and Jason W. Locasale^{1,2,*}

There has been a surge of interest in understanding the regulation of metabolic networks involved in disease in recent years. Quantitative models are increasingly being used to interrogate the metabolic pathways that are contained within this complex disease biology. At the core of this effort is the mathematical modeling of central carbon metabolism involving glycolysis and the citric acid cycle (referred to as energy metabolism). Here, we discuss several approaches used to quantitatively model metabolic pathways relating to energy metabolism and discuss their formalisms, successes, and limitations. © 2013 Wiley Periodicals, Inc.

How to cite this article:

WIREs Syst Biol Med 2013, 5:733–750. doi: 10.1002/wsbm.1238

INTRODUCTION

The accumulated amount of biochemical work carried out over the years has elaborated complex metabolic systems and networks. This information includes the network architecture encoded in chemical reactions that are carried out by metabolic enzymes and the kinetic parameters that determine reaction mechanisms involved in each of these chemical reactions. Application of this knowledge has led to tremendous predictive capability in characterizing metabolic regulation in normal physiology including the growth of unicellular organisms and the successful simulation of energy metabolism in healthy red blood cells. However, there are far fewer instances in which these models have been applied to the characterization of pathophysiology. Applying our knowledge of metabolic regulation to the investigation of disease states such as cancer or neurodegeneration is currently a scientific frontier. In this review, we will revisit several classic techniques for the mathematical modeling of metabolic pathways and discuss instances where their application to biomedical science is beginning to yield fruitful dividends.

*Correspondence to: locasale@cornell.edu

¹Division of Nutritional Sciences, Cornell University, Ithaca, NY, USA

²Tri-Institutional Field of Computational Biology and Medicine, Cornell University, Ithaca, NY, USA

Conflict of interest: The authors have declared no conflicts of interest for this article.

LINEAR SYSTEMS: FLUX BALANCE ANALYSIS

Linear models are mathematical models that contain a set of algebraic equations based on the stoichiometric relationships that define conservation relationships within a metabolic network. Linear models, to our knowledge, were first applied to biochemical systems in 1961 by Shapiro.¹ Shapiro discussed the possibility of using optimization in biochemical linear models in a 1969 publication.² In 1984, a model incorporating glycolysis and the tricarboxylic acid cycle (TCA) cycle was employed running a variant of Dantzig's algorithm with the assumed biological objective of minimized free energy dissipation.^{3,4} An enduring research program was initiated by Palsson half a decade later.^{5,6}

An early work of Edwards and Palsson showed that growth maximization in an *Escherichia coli* model could correctly match 86% of 79 gene essentialities examined.⁷ Subsequent modeling in *Saccharomyces cerevisiae* was able to closely predict growth rates and exometabolic fluxes in various media, and nearly capture the *in vivo* phosphate/oxygen (P/O) ratio of 0.94 with a simulated P/O value of 1.04, showing that models of eukaryotes were also feasible.⁸ If one chooses the biological objective function to reflect the appropriate physiological demands, then it is possible to predict features of adaptation; this was shown to be the case for growth optimization in several *E. coli* mutants.⁹

By this time it had become apparent that linear models held much promise, particularly when coupled with optimization.

Genome-Scale Modeling

Today, when we refer to linear models, we most often mean constraint-based models (CBMs). We refer to a CBM as any model making use of the stoichiometric matrix, S , as a linear matrix constraint, e.g., $S * F = 0$, where F is a flux vector. In fact, this is a nearly universal constraint, as it guarantees conservation of mass during steady-state processes such as exponential growth or tissue maintenance.¹⁰ Other constraints commonly used include reversibility constraints when the direction of a reaction is known for physiological conditions of interest, bounds on the uptake of nutrients or efflux rates due to regulation or physiology, or bounds on enzyme reactions when the maximum enzyme velocity V_{\max} is known.

Because these constraints give rise to an underdetermined system, it will not be possible to identify a unique solution for the flux vector. A unique solution is often desirable as it allows investigators to analyze a putative metabolic phenotype. Indeed, this is one of the more convenient features of linear optimization: the ability to get meaningful solutions without explicitly taking into account any, or at least very few, free parameters. Flux balance analysis (FBA) assumes a linear combination of fluxes to be maximized or minimized (Figure 1). In microbes, perhaps the most popular FBA objective has been growth maximization, which consists of the biomass precursors and products formulated as a single pseudo-reaction. Additionally, an ATP maintenance constraint should be formulated as a sink reaction with the molar ATP required to keep 1 g of dry weight biomass living for 1 h.¹¹ This empirically determined constraint, although assumed, is less discussed, perhaps owing to its dependence on individual strains and environments. We note that for many expression-based methods in the CBM framework, the ATP maintenance constraint is not required (see Table 1 and Figure 2 for examples). Fixed biomass objectives by themselves also have some undesirable qualities; biomass composition likely has some measure of variability based on genetic background and environment. Robust FBA attempts to address this problem by allowing some variation in the biomass composition, as determined by variation of empirical assays of biomass.¹² Despite these caveats, FBA has recently been found to not only predict growth in microbes but also has good agreement with gold standard ¹³C flux assays *in vivo*

when the growth objective is used along with ATP synthesis maximization and minimization of absolute fluxes.¹³

Minimization of absolute flux is a commonly used objective employed alongside other objectives, forming a minimax problem (i.e., finding the minimum absolute flux profile among all flux profiles that maximize biomass). This approximates the biological goal of being efficient with enzyme production costs and enzyme crowding constraints while also guaranteeing that no thermodynamically impossible loops are present, that is, ruling out some fluxes that might otherwise violate Kirchoff's loop rule.^{14,15} This constraint will work whenever a sink reaction, such as growth, is being optimized. However, maximizing an internal flux, as in flux variability analysis,¹⁶ could still result in internal cycles.¹⁵ Initial thermodynamic approaches involved nonlinear optimization.^{17–20} Constraints satisfying Kirchoff's loop rule were later developed that were faster and more generally applicable than prior methods.^{15,21} Still, these involve integer constraints that put this problem in a slower class of algorithms than the convex minimized absolute flux problem. When available, thermodynamic data is valuable; it can not only be used to guarantee that there are no internal cycles but can also aid in determining reaction direction and potential regulatory targets.^{15,18,22,23} Application of this framework to concentration data allows unmeasured metabolite concentrations to be inferred and global concentrations to be resolved at the organelle level.²⁰ CBMs have also found use in tracing individual atoms through pathways, which provide a more appealing framework for performing metabolic flux analysis (MFA; discussed below) on stable isotope data owing to the lack of bias compared with typical MFA models, which are often an order of magnitude smaller than genome-scale reconstructions.²⁴ Recent insightful work has made it possible to simplify the computational complexity of loopless FBA to be nearly the same as conventional FBA, but some mathematical difficulties must still be overcome before bounds on exchange fluxes can be suitably incorporated for genome-scale modeling.^{10,25}

The metabolism of different tissues within the same organism is diverse; whereas the metabolism in liver is anabolic, neurons or red blood cells have a much more limited catabolic regime.^{26–28} The creation of tissue-specific models for multicellular organisms has become an important problem, and several automated algorithms taking as inputs tissue expression data and a generic model for the organism have been developed.^{28–30} Coupling multiple cellular models together will enable multiscale modeling of

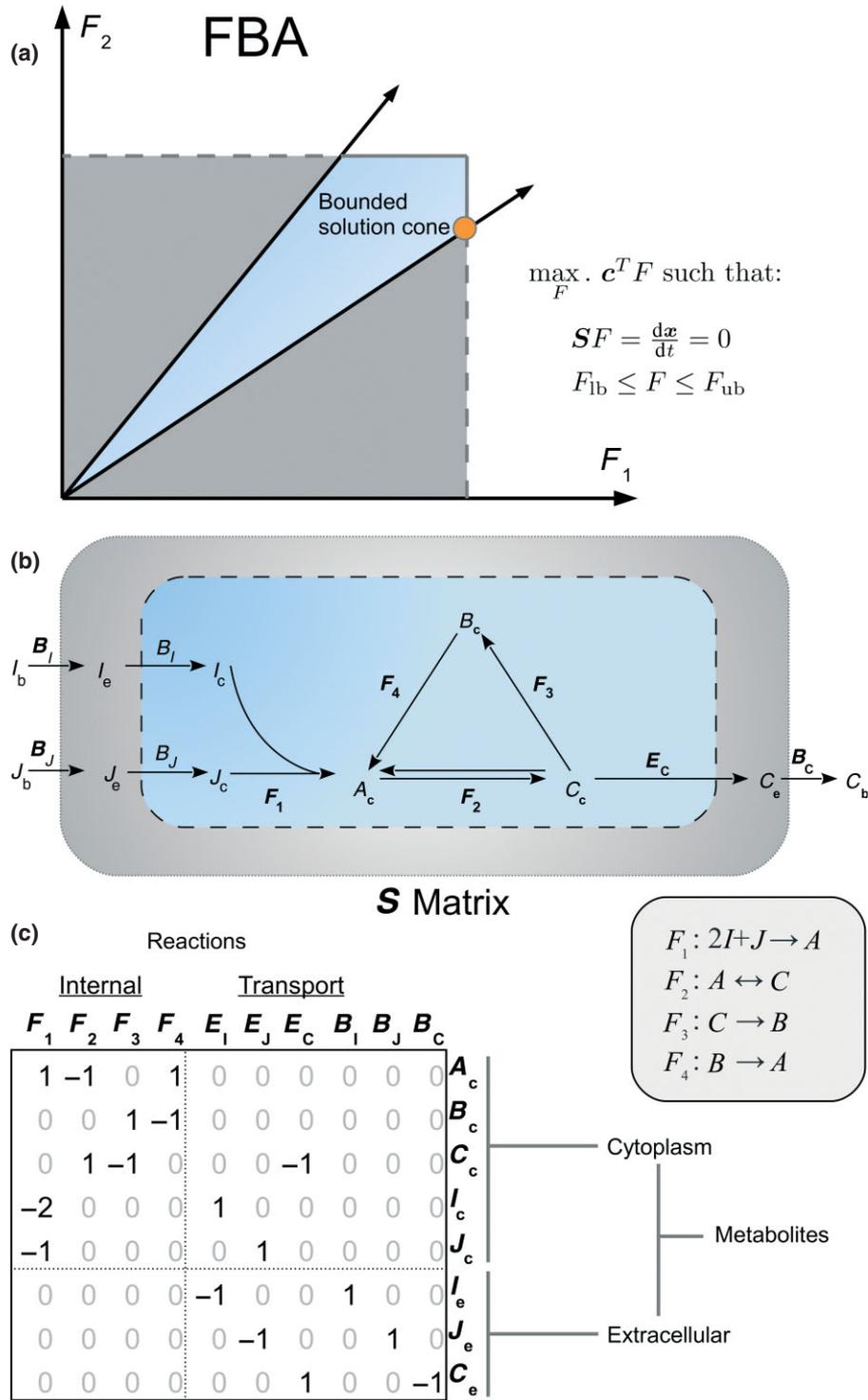


FIGURE 1 | (a) A simple geometric illustration of a flux balance analysis (FBA) problem. Constant constraints on the F_i limit the feasible solution to an n -dimensional cube (shown in gray). Further linear constraints from the S matrix create a cone of feasible solutions (blue). Linear programming algorithms find an optimal solution on a vertex (illustrated with orange circle). (b and c) Depiction of a simple metabolic network with compartmentalization and its associated stoichiometric matrix. The three compartments denoted with subscripts b, e, and c represent the boundary, extracellular environment, and cytosol, respectively. The boundary is what separates the model from its environment, and mass balance is not assumed at the boundary; this allows for the implementation of source and sink reactions.

TABLE 1 | Families of Methods for Constraint-Based Models

Method Family	Description	Benefits	Caveats	Solver Type	Notes	Refs
FBA	Flux balance analysis: linear programming applied to the model	Usually very fast and simple to use, especially when a biomass pseudo-objective is available	Arguably has more limited use in nonmicrobial models. Only simple objectives or sequential (e.g., bilevel) optimization is practical	Linear	Often constraint-based modeling (CBM) in general may be referred to as FBA, though this is not technically correct	16
MoMA	Minimization of metabolic adjustment	Usually very fast and simple to use, especially when a reference or wild-type flux is available; useful for simulating mutations	It has been argued that the closest distance to a flux does not represent mutation as well as simulating the least number of flux changes (ROOM)	Linear, quadratic convex	Related, but slightly more sophisticated methods are being used to estimate flux profiles from expression data	46, 47
DFBA	Dynamic FBA: incorporates a step-wise simulation of FBA, along with update rules that relate biomass to uptake rate, solving for extracellular concentrations	Allows for some non-steady-state observations	Small timescale dynamics and intracellular dynamics may be difficult to model	Linear (iterative)	Other, but infrequently used (owing to difficulty) methods involving regulation (rFBA) or multiscale models of tissues build on this approach	11
EBA	Energy balance analysis: FBA, but also incorporates thermodynamic constraints	Incorporates thermodynamic information and prevents futile cycles	Usually much slower than LP methods like FBA	Nonlinear, MILP, or monotropic	A highly active research area	10, 15, 17, 19

TABLE 1 | Continued

Method Family	Description	Benefits	Caveats	Solver Type	Notes	Refs
Tissue-specific model creation	Requires expression data for tissue of interest	Tissues have vastly different regulatory schemes; these methods take this into account by finding which metabolic genes are likely to be expressed in a given tissue	Still requires some other method and objective to estimate flux or do pathway analysis	MILP	A highly active research area	28–30
Expression-flux mapping	Takes ideas from MoMA and tissue-specific model creation to estimate fluxes	Unlike tissue-specific models, will actually estimate the flux as a MoMA-like objective is employed	Requires high-quality (e.g., RNA-seq) expression data, or for PROM, abundant microarray data from different conditions	Linear optimization, but moderate number of simulations or preprocessing required	Highly accurate predictions can be obtained	48, 49
Interaction search	Epistasis, or genetic interactions, come up in many contexts, but are also important in energy metabolism, as energy is often related to very important phenotypes including growth, proliferation, and survival	For such analyses, convex optimization may offer the only tractable method	Simulating pairwise epistasis in the general case requires pairwise simulation of all double mutants of interest, which can be very time consuming at the genome scale when different mutations in each gene, or different environments, are considered	Linear optimization, but often many simulations required. Min cuts (exponential)	The sign of weak epistasis is difficult to predict owing to error propagation in growth rates	50–53

Broad classes of methods are described, along with references to some individual implementations or studies.

to generate owing to the necessity of protein localization and metabolite transporter information.³⁴ Automatic reconstruction going beyond enzymatic gene information, such as regulatory FBA (rFBA) models, should also be possible,^{40,41} the automated generation of Boolean and higher order discrete regulatory models using time-series expression data has been explored as well, although to date these regulatory models have not been coupled to metabolic reconstructions.^{42–45} These approaches and other families of genome-scale methods are discussed in Table 1.

Several approaches have been used in applying CBMs to cancer and the Warburg effect, the preference for glycolytic ATP production over glucose-derived mitochondrial ATP production in cancer cells.^{54–56} An important study working with a simplified model of central carbon metabolism showed that, while the TCA cycle predicts better ATP yield than glycolysis when only available glucose is considered as a constraint, the addition of enzyme solvent-capacity constraints creates a preference for ATP synthesis through glycolysis.⁵⁶ More recently, the work of Vazquez and Oltvai was extended to include a genome-scale model along with enzyme solvent-capacity constraints, which was able to show significant correlations between fluxes and expression in the NCI-60 cell line panel, as well as predicting an intermediate state in cancer metabolism transition exhibiting a temporary increase in OxPhos that was supported by two prior experimental observations.⁵⁵ Each of these approaches correctly predicted lactate production. Concurrent research on predicting cancer targets was carried out by screening for simulated negative epistasis in cancer tissue-specific models that have at least one known-drug target and no known effect on normal tissue revealed many epistatic interactions.³⁹ A related study confirmed one of these synthetic lethalties between heme oxygenase and fumarate hydratase, a mutation found in certain kidney cancers.⁵⁷ The recent publication of Human Recon 2 promises to aid in the understanding of many human diseases; already 65 cell-type-specific models based on it are available, and the model reports 77% accuracy in identifying metabolic markers across 49 inborn errors of metabolism.⁵⁸ Although this model is a great step forward in consolidating much of the knowledge about human metabolism, it is only one of many steps to come. For instance, this model is still primarily only amenable to steady-state approaches, lacks corresponding enzyme-regulatory and signaling architecture, and has introduced more dead-end metabolites than it removed (1176 vs 339).

Conclusions

Kinetic models for smaller pathways are possible when the data are present, but many energetic questions concern the entire cell, leaving only incorporation of CBMs as a viable option. The original efficiency and ease of use of FBA have helped propagate a field of more diverse algorithms that are often tractable on today's computers using the same modeling and software frameworks.^{59,60} Numerous methods and successful applications in energy metabolism exist, including prevalent diseases such as heart disease, cancer, and Alzheimer's.⁶¹

Multiscale models, as were used in the Alzheimer's models, will undoubtedly become more common. At the intracellular scale, CBMs are also beginning to incorporate information other than metabolic stoichiometry.^{62–64} A whole-cell model for *Mycoplasma genitalium* incorporating information about all classes of macromolecular synthesis and degradation, in addition to stoichiometric and regulatory information, found a nonstochastic coupling between metabolism and the cell cycle where DNA replication rates depended on the concentration of dNTP.⁶³ Models like these are not easy to build, but substantial endeavors are underway to assist in their draft construction and refinement, and together with an increase in use of jamboree meetings of organism and model experts and online collaborative tools, and will likely aid in creating public models of higher quality and the understanding of many biological processes outside the traditional scope of metabolism.^{35,58,65–69}

BIOCHEMICAL KINETIC MODELING

Biochemical kinetic models describe dynamic properties of metabolic and signaling networks, predicting a variety of different properties, e.g., fluxes, metabolite concentrations or complex dynamic behavior with multiple steady states, oscillations, and bifurcations⁷⁰ (Figure 2). These kinetic models form mechanistic descriptions of metabolic networks and are able not only to predict effects of environmental stresses or genomic changes but also allow for the investigation of network robustness and design principles. To generate such a model, kinetic parameters must be included in the model explicitly. In practice, this requirement makes such models substantially underdetermined. As a result, extensive parameter sensitivity evaluations are required for all model calculations. In this section, we discuss the basic formalism of kinetic models. Because of space limitations we do not consider here some important strategies such as parameter estimation, model validation, and other types of analysis of

network models and instead we refer to approaches reviewed recently.^{71,72}

Kinetic Models of Metabolic Networks

To construct kinetic models, several types of data are required. A component of all metabolic networks is stoichiometry and this was discussed above (stoichiometric matrix S ; see also FBA part, Eq. (1)).

$$\frac{dM}{dt} = S * F(M, p), \quad (1)$$

where S is the stoichiometry matrix, M and F are the concentration and flux vectors, and p is the parameter vector.

Presently, metabolic pathway charts are known for many organisms and tissues and there are several databases containing this information, e.g., KEGG metabolic pathways database (see Box 1). Construction of models requires the use of mechanistic enzyme flux equations and their reaction laws. The reaction rate (F , Eq. (1)) depends on the concentration of metabolites and kinetic/thermodynamic parameters: V_{\max} , the maximum activity of the enzyme, turnover rates, Michaelis–Menten constants, effector constants, and others. There is a lot of literature available for enzyme kinetics.^{73,74} A limiting factor in construction of complex dynamic models is the lack of knowledge of kinetic mechanisms and the difficulty in experimental identification of parameters. So, the common strategy in computational biology is to reduce the number of unknown parameters and consequently to use simplified or generic rate equations.^{75,76} Another alternative modeling approach, hybrid dynamic modeling, combines detailed mechanistic kinetics for regulatory enzymes with simplified rate equations with a small number of parameters for the remaining reactions.^{77,78} To check the reliability of this approach, Bulik et al.⁷⁸ have applied it to two independent metabolic networks including one involving energy and redox metabolism of red blood cells. Calculations of stationary and temporary states under various physiological challenges demonstrate the good performance of the hybrid models.

Constructions of dynamic models with multi-level hierarchical networks that include the integration of multiple biological processes including metabolism, signal transduction, genetic regulation,⁸⁷ and even living whole cell⁶³ have also been carried out.

All enzyme-catalyzed reactions are reversible in principle and thermodynamic constraints have to be captured in kinetic modeling. There are several thermodynamic databases for enzymatic reactions available (see Box 1). Several databases have been

developed for enzyme kinetic data such as BRENDA and SABIO-RK (see Box 1). In 2004, the STRENDA (STandards for Reporting Enzymology DATA)—a Commission of Beilstein-Institut in Germany, was setup to develop standardization of enzyme data. The STRENDA commission is accompanied by ESCEC (Experimental Standard Conditions of Enzyme Characterizations) conferences where the latest in enzymology and systems biology is presented. Other databases are also described in Box 1.

BOX 1

ONLINE RESOURCES FOR KINETIC MODELING

Enzymes, Pathways, and Metabolites

KEGG (Kyoto Encyclopedia of Genes and Genomes): Comprehensive metabolic pathways database dealing with genes, protein, metabolites, and pathways (<http://www.genome.jp/kegg/>)

BRENDA (BRaunschweigENZymeDAtabase): Extensive enzyme database⁷⁹ (<http://www.brenda-enzymes.org/>)

SABIO-RK (System for the Analysis of BIOchemicalpathways-Reaction Kinetics): Extension of SABIO biopathway database developed for biochemical reaction kinetics⁸⁰ (<http://sabio.h-its.org/>)

STRENDA: Standards for Reporting Enzymology Data (<http://www.beilstein-institut.de/en/projects/strenda/>)

GTD: The Thermodynamics of Enzyme-Catalyzed Reactions database, the National Institute of Standards and Technology (NIST, USA)⁸¹ (http://xpdn.nist.gov/enzyme_thermodynamics/)

ExplorEnz: A database of the IUBMB enzyme list⁸² (<http://www.enzyme-database.org/index.php>)

ExpASy: Enzyme nomenclature database (<http://enzyme.expasy.org/>)

MetaCyc: A database of experimentally elucidated metabolic pathways⁸³ (<http://metacyc.org/>)

HMDB: The Human Metabolome Data Base—contains detailed information about small-molecule metabolites found in the human body⁸⁴ (<http://www.hmdb.ca/>)

Metabolic Modeling

SBML (Systems Biology Markup Language). A biomodels database for storing computational models of bioprocesses (http://sbml.org/Main_Page)

GEPASI: Popular software package for kinetic metabolic analysis⁸⁵ (<http://www.gepasi.org/gepasi.html>)

Cellware: Modeling tool for cellular transactions (<http://www.bii.a-star.edu.sg/achievements/applications/cellware/index.php>)

BISEN: Biochemical Simulation Environment—set of tools for generating equations for simulating biochemical systems in the Matlab (bbc.mcw.edu/BISEN)⁸⁶

COPASY: A software for simulation and analysis of biochemical networks (http://www.copasi.org/tiki-view_articles.php)

DIZZY: Chemical kinetics stochastic simulation software (<http://systems-biology.org/software/simulation/dizzy.html>)

Modeling of metabolic dynamics from the cellular to organ level is a powerful tool for interpreting experimental data. Recently, several kinetic models at the organ level were developed to study energy metabolism in brain,^{88–90} muscle,^{75,76} and heart.^{91,92} These modeling approaches allow for the evaluation of the relative significance of metabolic pathways and regulatory mechanisms, and the prediction of responses to environmental stimuli that cannot be directly measured such as the introduction of a drug. These models are also being applied to bioenergetics of diseases such as Parkinson's disease.⁹³

Sensitivity Analysis and Metabolic Control

Mechanism-based models predict dynamics in a specified system for each set of determined system parameters. However, it is important to further investigate the effect of parameter perturbations on the overall system. Identification of network control points, robustness, and parameter sensitivities is most crucial to the prediction of the system output behavior. Local parameter sensitivity analysis has been used to identify critical parameters in dynamic models of, e.g., muscle energetics⁷⁶ and excitable cell ATP dynamics.⁹⁴ The local sensitivity coefficient is defined as:

$$S_p^R = \left(\frac{\partial R/R}{\partial p/p} \right)_{ss},$$

where p represents the parameter that is varied, R is a response of the system output such as a concentration or flux, and subscript ss means differentiation at steady state. Local sensitivity analysis allows only one parameter to vary for each calculation, deals

with small perturbations, and is most widely used in metabolic systems.⁷⁰ However, parameters can vary extensively, and for this reason it is more appropriate to explore the possibility of nonlinear effects from simultaneous variations of arbitrary magnitude by means of global parameter sensitivity analysis (GSA).^{71,95} GSA has the advantage that it allows for a more comprehensive analysis by applying a Monte-Carlo strategy to sample distributions of random parameters.⁹⁵ For each parameter set the sensitivity indices are calculated by minimization of an objective function, defined as a sum of squared errors between perturbed and reference or experimental output.⁹⁵

Metabolic control analysis (MCA) is a form of sensitivity analysis that is used in metabolic engineering. MCA computes the extent to which an enzyme controls a flux or concentration in the network. Control coefficients describe the relative sensitivities of dependent variables to independent system parameters. MCA helps to elucidate the distribution of concentration and flux control coefficients (FCCs). This approach was developed independently by two groups in the seventies.^{96,97} In particular, control coefficients describe the change in system variables as a result of perturbation of particular enzyme concentrations (independent parameter). The magnitude of change in pathway flux in response to enzyme concentration change is expressed as the FCC⁹⁷

$$C_{E_i}^F = \left(\frac{\partial F/F}{\partial E_i/E_i} \right)_{ss} = \left(\frac{\partial \ln F}{\partial \ln E_i} \right)_{ss}, \quad (2)$$

where $C_{E_i}^F$ is the FCC of the i th enzyme, F is the steady-state flux, E_i is the activity of i th enzyme, and the subscript ss means differentiation at the new steady-state condition. One feature of MCA is that control properties result from log–log derivatives. As a result, summation theorems state that, e.g., for FCC the sum of all FCCs in the metabolic network is equal to 1.⁹⁷

Although sensitivity analysis is widely used in kinetic modeling, it is rarely used in genome-scale modeling techniques such as FBA. This is despite the fact that early publications discuss the notion of shadow prices, which describe the rate of change in the objective function with respect to a particular flux, as well as prominent toolboxes featuring implementations of MCMC sampling strategies.^{5,98}

Conclusions

In summary, mechanism-based kinetic models, though applied to limited bionetworks, provide a thorough understanding of biological systems. To understand

dynamic features of metabolic networks, parameter fits are not necessary, especially when experimental data is limited or not available. In these regards, sensitivity analysis becomes a significant tool to study dynamic flux control and has the potential to develop models that possess prognostic power.⁷¹

STABLE ISOTOPE TRACING AND MFA

MFA employs stable isotope tracing and aims to characterize fluxes based on the distribution of labeling patterns of heavy isotopes (most commonly ¹³C) that are introduced into cells. MFA can yield novel insight into the operation of biological systems, e.g., discovering features such as network mechanisms, novel pathways, futile cycles (substrate cycling), or alternative reactions. A large set of fluxes in a flux map is described as a fluxome and was defined by Sauer et al.⁹⁹ as the array of fluxes for all the reactions in a living system. The field of fluxomics aims to analyze this set of fluxes⁹⁹ (see Figure 2). In metabolome-wide MFA the number of measurements from labeling experiments is usually much larger than the number of fluxes to be determined. This makes flux estimation an overdetermined problem in mathematical terms. The challenges of modern MFA have provided the motivation to develop additional theoretical frameworks to study the fluxome. For example, the details of flux analysis based on cumomers (see Boxes 2 and 3) are explained in series of articles.^{100–102} Alternative methods such as elementary metabolite units¹⁰³ and bonded cumomers¹⁰⁴ aim to minimize the number of necessary state variables and to reduce computational cost.^{105,106}

BOX 2

GLOSSARY FOR MFA

Isotopomer (or sometimes refer as isotopologue): 'Isotopic' molecule that represents one possible labeled state of a given substrate and so differing in position of isotopes. For metabolite *M* with *n* different carbon atoms there are 2^n possible isotopomers (if labeled with two isotopes, e.g., ¹²C or ¹³C isotopes). Particular isotopomer *M*(*i*₁, *i*₂...*i*_n) is the isotopomer with labeled atoms in *i*₁, *i*₂ positions. For example, the Glu(1,2) isotopomer of glutamate is labeled with its first and second carbon atoms and all other atoms are unlabeled.

Mass isotopomer: A set of isotopomers with the same mass. For instance, the mass-isotopomer alanine *M*+2 (*AlaM*₂) contains all

isotopomers with two labeled atoms. A molecule with *n* carbon atoms has *n* + 1 mass isotopomers.

Cumomer: The set of isotopomers of metabolite *M* that contain a particular labeled fragment,¹⁰⁰ thus representing a 'virtual' isotopic molecule. Cumomer *M*[*i*₁, *i*₂...*i*_k] is the set of isotopomers with labeled *i*₁, *i*₂...*i*_k atoms. For example, *Lac*[1,2] cumomer of lactate with labeled first and second atoms and the third atom is either labeled or unlabeled. Total number of cumomers for molecule with *n* different carbon atoms equals to total number of isotopomers, 2^n .

Bonded cumomer: Cumomer whose indices refer to adjacent carbons.¹⁰⁴ *Lac*[1,2]-bonded cumomer and *Lac*[1,3] nonbonded.

Flux (*F*): Rate of reaction, expressed, e.g., in mkmol/g/min. Reflect *in vivo* enzymes activity and pathways rate. Flux information is important for mechanistic metabolic and disease pathophysiology studies.

Net flux: Difference between reaction forward and backward fluxes $F_f - F_b$.

Exchange flux (*F_e*): Often referred as a minimal flux between forward or backward fluxes, usually when $F_f \geq F_b$, $F_e = F_b$ (see above).

Fluxome: Set of fluxes for the reactions in organism network. The term was introduced by Sauer et al. in 1999.⁹⁹

Fluxomics: The discipline that applies different computational methods to analyze fluxome.

FBA family: Steady-state analysis of fluxes, based, e.g., on measured input and output (transport) fluxes or whole gene, protein expression, and linear programming.

MFA: Steady-state or dynamic analysis of fluxes based on the network stoichiometry and on the redistribution of labeled patterns of metabolites.

These fluxomics methods are classified as dynamic or static (steady state) depending on the manner of measurement of labeled metabolite patterns. Isotope-based MFA has been applied successfully to complex bionetworks with metabolic cycles, subcellular compartmentalization, reaction reversibility, and futile substrate cycling. Recently, MFA has become a widely used tool. The general methodology for both isotopically steady state and dynamic approaches for ¹³C MFA and ¹³C metabolic modeling has been reviewed recently, with applications to mammalian physiological systems (e.g., brain),^{114,116–119} microbial fluxome,^{120,121} and

plants.¹²² Some important problems in MFA including its methodology, flux error analysis, and model validation are discussed elsewhere.^{116,123}

BOX 3

ONLINE RESOURCES FOR ¹³C MFA AND FBA

OpenFLUX: Software for ¹³C-based MFA¹⁰⁷
¹³*CFLUX*: Software package for analyzing steady-state ¹³C labeling experiments; runs under Linux¹⁰⁸ (<https://www.13cflux.net/13cflux/>)

IMS2Flux: MS data processing tool for isotope labeling experiments focusing on increasing throughput at multiple stages of the data analysis¹⁰⁹ (<http://sourceforge.net/projects/ims2flux/>)

¹³*CFLUX2*: The new high-performance software suite for ¹³C-MFA; runs under Linux¹¹⁰ (<http://www.13cflux.net/13cflux2/>)

FiatFlux: A software for MFA from ¹³C-glucose experiments¹¹¹

ETA: Extracellular time-course analysis, MATLAB-based software for determination of cell-specific rates from extracellular time courses.¹¹²

NMR2Flux: Software tool developed for plant metabolism based on two-dimensional NMR spectra¹¹³

CWave: Software package designed for dynamic ¹³C MFA with positional enrichments based on *in vivo* NMR data.¹¹⁴

COBRA Toolbox: Open-source MATLAB and Python packages for use with genome-scale models, which includes implementations of many of the linear and constraint-based algorithms discussed in this review⁹⁸ (<http://opencobra.sourceforge.net/openCOBRA/Welcome.html>)

BioMet: Web-based toolbox for stoichiometric analysis provides the capabilities of genome-wide analysis of metabolism¹¹⁵ (www.sysbio.se/BioMet/)

In Silico Organisms: A well-maintained list of curated genome-scale reconstructions and models (<http://cgcr.ucsd.edu/InSilicoOrganisms/OtherOrganisms>)

COBRA Methods: A fairly comprehensive list of genome-scale methods (<http://cobramethods.wikidot.com/methods>)

MFA currently represents one of the most powerful fluxomics techniques to estimate network

fluxes, allowing estimation of both net and exchange fluxes within multicellular and subcellular compartments (Figure 2). MFA differs from FBA by incorporating the data from experiments using isotope-labeled nutrients (i.e., a tracer) into a metabolic model, and in general is a nonlinear problem. Tracers are supplied continuously to a biological system at metabolic steady state and labeling patterns of downstream metabolites are analyzed. However, it is possible to feed tissue or cells with a limited quantity of label, e.g., with a bolus or pulse, and this infusion technique is relatively common in physiological *in vivo* temporal studies.¹¹⁴ The propagation of labels through a network depends on the network's structure, activity of network enzymes (fluxes), and pool sizes; larger pools slow down propagation and higher fluxes accelerate it.¹¹⁶

Isotopic enrichments or patterns in metabolites are usually measured by mass spectrometry (MS) coupled with liquid chromatography (LC), gas chromatography (GC) and NMR. The isotopes most often used to study bioenergetics are ³¹P (e.g., brain ATP rate analyzed by NMR),^{124,125} ¹⁷O (e.g., cerebral oxygen metabolism by NMR),^{125,126} ¹⁸O (whole-body energy balance by MS),¹²⁷ ²H (e.g., lactate recycling by NMR),¹²⁸ and most commonly ¹³C (see above, NMR and MS). The ability to use NMR spectroscopy to study energy metabolism was demonstrated for ³¹P¹²⁹ and for ¹³C^{130,131} using suspension cultures of microorganisms. Thereafter, seminal *in vivo* kinetics studies of energy metabolism have been made with ¹³C in perfused heart^{132,133} and liver,^{134–136} and noninvasively in brain^{137,138} and skeletal muscle^{139,140} using different models.

Technological advances in NMR and MS have led to advances in metabolomics.¹⁴¹ In parallel, analytical techniques for ¹³C MFA have been developed—from relatively simple to complex multicompartmental models with extended bionetworks represented by large numbers of equations. These models were able to demonstrate that human brain energy metabolism has not only a neuronal but also glial component, and have further shown that in glia, TCA cycle and anaplerotic pyruvate carboxylase activity are significant,¹⁴² and that neuronal TCA cycle activity increases during visual stimulation¹⁴³ and decreases during normal aging, leading to a neuronal loss of oxidative capacity.¹⁴⁴

Both NMR and MS are capable of measuring label distribution in glycolysis and TCA cycle-associated intermediates. High-resolution LC-MS methods allow for the assessment of all mass isotopomers ($n + 1$ in total for a metabolite with n carbon atoms, Box 2) of glycolytic and TCA cycle

intermediates, many of which are not detectable by NMR owing to low sensitivity. However, NMR gives more specific information about metabolites' positional enrichments via its analysis of ^{13}C multiplet spectra (e.g., *Glut4*-glutamate labeled at C4 position and other amino acids associated with TCA cycle glutamine and aspartate). Still, even this technique is not able to quantify all possible molecules that differ only in their isotope distribution (i.e., isotopomers, see Box 2) ($=2^n$ for a molecule with n different carbon atoms) with one exception.¹⁴⁵ Therefore, the combination of both methods could potentially give more valuable metabolic information about bionetworks and better precision for calculated fluxes.

High sensitivity could favor the use of radioisotopes [analyzed by liquid scintillation counting and/or positron emission tomography (PET)] and ^{13}C hyperpolarized compounds for flux studies. They are particularly convenient if there is no need for positional labeling information. An interesting use of ^{11}C isotope with PET and a mathematical model to study neuroenergetics was recently published.¹⁴⁶

Detailed mathematical models are required for the correct interpretation of experimental data and to analyze isotopic patterns to calculate *in vivo* fluxes. Metabolic models differ depending on isotopic specificity of the input data, but three families can be distinguished: positional models, mass-isotopomer models, and isotopomer models (see Figure 2). Most metabolic labeled experiments are limited to measurement of positional fractional enrichments of metabolites (in the case of ^{13}C NMR, the yield is at most n independent variables for a metabolite with n asymmetrical carbon atoms) and to only one or few mass isotopomers from all MS data ($n + 1$ mass isotopomers). As a consequence, there has been no complete description of isotopomer distribution dynamics, resulting in the loss of a lot of mechanistic biochemical information and the reliable determination of metabolic parameters. The main targets of modern isotopomer modeling approaches relate to the accurate determination of metabolic fluxes, improving their reliability and providing maximal metabolic information that can be derived from the fine structure of ^{13}C NMR spectroscopy of metabolites and/or metabolome-scale ^{13}C mass-isotopomer distributions (Box 3)

CONCLUSIONS

Various approaches for MFA have been employed recently, with the most advanced being cumomer modeling. Despite these advances in the theoretical basis for MFA, it is still an expanding and very active research field. Further progress will combine different

analytical and experimental techniques, e.g., MS and NMR data with advanced dynamic and steady-state MFA techniques capable of handling heterogeneous data.

There is a significant value for MFA in many biomedical fields. High-performance 'omics' tools expand the application of flux analysis further to understand *in vivo* metabolism and its mechanisms and regulation under different conditions, elucidating the pathological mechanism of diseases, providing information on bottleneck reactions, and identifying specific steps for drug targets. Moreover, by providing information on flux in individual cells and tissues, MFA can significantly expand the potential of 'omics' techniques.

SUMMARY

Fluxes through metabolism directly report *in vivo* enzyme reaction rates. To comprehensively understand metabolism and elucidate its regulation all three flux modeling approaches should be applied. Each of these modeling approaches (linear modeling, kinetic modeling, and MFA) has successes and limitations. There have been a variety of successes in modeling energy metabolism with steady-state techniques, from the better understanding of diseases as diverse as Alzheimer's disease and host-pathogen diseases to predicting treatments for cancer. Despite such amazing successes, it must be cautioned that these models are far from perfect; 77% of metabolic biomarkers for inborn errors in metabolism can be predicted with correct directionality with the recently published Human Recon 2, and while a great achievement, still leaves much room for improvement. The yeast models, which have also shown much promise in predicting many phenotypes, have difficulty when predicting effects requiring greater precision, such as epistasis. Undoubtedly, this is largely due to the incompleteness of the reconstructions themselves. For several of the more popular model organisms, iterative improvements of reconstruction releases remain an active area of research. Other model organisms, such as *Drosophila melanogaster*, a model organism often used for studying mitochondrial defects, do not yet possess even a draft reconstruction. The parallel advances in modeling techniques enable the reconstructions to serve a dually important role as mathematically and experimentally verified databases; errors can easily be found by computational procedures, showing us where more experiments are needed to fill the gaps.

A limitation of linear models themselves is their inability to simulate dynamics. But, this is a somewhat

artificial constraint, as integrated techniques utilizing the same reconstructions have proven to be successful. Increasingly, integrated techniques and diverse types of data underlying organism or cellular modeling will also play a vital role in improving predictive capability and a systematic knowledge base for biology. When trying to study individual or small sets of pathways, kinetic models may be relatively easy to implement if data is available, and data is rapidly becoming easier to generate with advances in mass spectrometry.

However, for many investigators, these methods may be neither easy to implement nor affordable to generate. Genome-scale models can cover more genes, with typically faster simulation times, making them particularly attractive to course-drained drug prediction or genetic interaction studies. In both cases, accuracy largely depends on the assumptions made by the user. Just because genome-scale methods such as FBA can be accurate and easy to run, does not mean a naive attempt will provide valuable predictions.

ACKNOWLEDGMENTS

The authors would like to thank members of the Locasale lab for helpful discussions and Yiping Wang for reading the manuscript. JWJ also thanks Marcin Imielinski for stimulating discussions on flux balance analysis. The authors gratefully acknowledge support from the American Cancer Society, Cornell University, the National Institutes of Health (CA168997 to JWJ), and the National Science Foundation (MCB-1243588 to ZG).

REFERENCES

1. Shapiro HM. Studies in the structure of the bacterial economy: an input-output model of *Escherichia coli*. Bachelor's Thesis. Department of Biochemical Sciences, Harvard University. 1961.
2. Shapiro HM. Input-output models of biological systems: formulation and applicability. *Comput Biomed Res* 1969, 2:430–445.
3. Van de Panne C, Rahnamat F. The first algorithm for linear programming: an analysis of Kantorovich's method. *Econ Plann* 1985, 19:76–91.
4. Watson MR. Metabolic maps for the Apple II. *Biochem Soc Trans* 1984, 12:1093–1094.
5. Savinell JM, Palsson BØ. Network analysis of intermediary metabolism using linear optimization. I. Development of mathematical formalism. *J Theor Biol* 1992, 154:421–454.
6. Savinell JM, Palsson BØ. Network analysis of intermediary metabolism using linear optimization. II. Interpretation of hybridoma cell metabolism. *J Theor Biol* 1992, 154:455–473.
7. Edwards JS, Palsson BØ. The *Escherichia coli* MG1655 in silico metabolic genotype: its definition, characteristics, and capabilities. *Proc Natl Acad Sci U S A* 2000, 97:5528–5533.
8. Famili I, Forster J, Nielsen J, Palsson BØ. *Saccharomyces cerevisiae* phenotypes can be predicted by using constraint-based analysis of a genome-scale reconstructed metabolic network. *Proc Natl Acad Sci U S A* 2003, 100:13134–13139.
9. Fong SS, Palsson BØ. Metabolic gene-deletion strains of *Escherichia coli* evolve to computationally predicted growth phenotypes. *Nat Genet* 2004, 36:1056–1058.
10. Fleming RMT, Maes CM, Saunders MA, Ye Y, Palsson BØ. A variational principle for computing nonequilibrium fluxes and potentials in genome-scale biochemical networks. *J Theor Biol* 2012, 292: 71–77.
11. Varma A, Palsson BØ. Stoichiometric flux balance models quantitatively predict growth and metabolic by-product secretion in wild-type *Escherichia coli* W3110. *Appl Environ Microbiol* 1994, 60:3724–3731.
12. Zavlanos, M. M. & Julius, A. A. Robust flux balance analysis of metabolic networks. *American Control Conference*, San Francisco, CA; 2011, 2915–2920.
13. Schuetz R, Zamboni N, Zampieri M, Heinemann M, Sauer U. Multidimensional optimality of microbial metabolism. *Science* 2012, 336:601–604.
14. Smallbone K, Simeonidis E. Flux balance analysis: a geometric perspective. *J Theor Biol* 2009, 258:311–315.
15. Schellenberger J, Lewis NE, Palsson BØ. Elimination of thermodynamically infeasible loops in steady-state metabolic models. *Biophys J* 2011, 100:544–553.
16. Orth JD, Thiele I, Palsson BØ. What is flux balance analysis? *Nat Biotechnol* 2010, 28:245–248.
17. Beard D, Liang S, Qian H. Energy balance for analysis of complex metabolic networks. *Biophys J* 2002, 83:79–86.
18. Henry CS, Jankowski MD, Broadbelt LJ, Hatzimanikatis V. Genome-scale thermodynamic analysis of *Escherichia coli* metabolism. *Biophys J* 2006, 90:1453–1461.

19. Henry CS, Broadbelt LJ, Hatzimanikatis V. Thermodynamics-based metabolic flux analysis. *Bio-phys J* 2007, 92:1792–1805.
20. Kümme A, Panke S, Heinemann M. Putative regulatory sites unraveled by network-embedded thermodynamic analysis of metabolome data. *Mol Syst Biol* 2006, 2:2006.0034.
21. Müller AC, Bockmayr A. Fast thermodynamically constrained flux variability analysis. *Bioinformatics* 2013, 29:1–7. doi: 10.1093/bioinformatics/btt059.
22. Haraldsdóttir HS, Thiele I, Fleming RMT. Quantitative assignment of reaction directionality in a multicompartimental human metabolic reconstruction. *Biophys J* 2012, 102:1703–1711.
23. De Martino D, Figliuzzi M, De Martino A, Marinari E. A scalable algorithm to explore the Gibbs energy landscape of genome-scale metabolic networks. *PLoS Comput Biol* 2012, 8:e1002562.
24. Ravikirithi P, Suthers PF, Maranas CD. Construction of an *E. coli* genome-scale atom mapping model for MFA calculations. *Biotechnol Bioeng* 2011, 108:1372–1382.
25. Warren P, Jones J. Duality, thermodynamics, and the linear programming problem in constraint-based models of metabolism. *Phys Rev Lett* 2007, 99:108101.
26. Lewis NE, Schramm G, Bordbar A, Schellenberger J, Andersen MP. Large-scale in silico modeling of metabolic interactions between cell types in the human brain. *Nat Biotechnol* 2010, 28:1279–1285.
27. Jamshidi N, Palsson BØ. Systems biology of the human red blood cell. *Blood Cells Mol Dis* 2006, 36:239–247.
28. Wang Y, Eddy JA, Price ND. Reconstruction of genome-scale metabolic models for 126 human tissues using mCADRE. *BMC Syst Biol* 2012, 6:153.
29. Becker SA, Palsson BØ. Context-specific metabolic networks are consistent with experiments. *PLoS Comput Biol* 2008, 4:1–10.
30. Shlomi T, Cabili MN, Herrgård MJ, Palsson BØ, Rupp E. Network-based prediction of human tissue-specific metabolism. *Nat Biotechnol* 2008, 26:1003–1010.
31. Sun Y, Fleming RMT, Thiele I, Saunders MA. Robust flux balance analysis of multiscale biochemical reaction networks. 2012:1–6. Available at <http://www-leland.stanford.edu/group/SOL/multiscale/papers/robustFba.pdf>
32. Bordbar A, Lewis NE, Schellenberger J, Palsson BØ, Jamshidi N. Insight into human alveolar macrophage and *M. tuberculosis* interactions via metabolic reconstructions. *Mol Syst Biol* 2010, 6: 422.
33. Klitgord N, Segrè D. Ecosystems biology of microbial metabolism. *Curr Opin Biotechnol* 2011, 22:541–546. doi: 10.1016/j.copbio.2011.04.018.
34. Seaver SMD, Henry CS, Hanson AD. Frontiers in metabolic reconstruction and modeling of plant genomes. *J Exp Bot* 2012, 63:2247–2258.
35. Aziz RK, Devoid S, Disz T, Edwards R, Henry CS. SEED servers: high-performance access to the SEED genomes, annotations, and metabolic models. *PLoS One* 2012, 7:e48053.
36. Henry CS, Overbeek R, Xia F, Best AA, Glass E. Connecting genotype to phenotype in the era of high-throughput sequencing. *Biochim Biophys Acta* 2011, 1810:967–977.
37. Faria JP, Overbeek R, Xia F, Rocha M, Rocha I. Genome-scale bacterial transcriptional regulatory networks: reconstruction and integrated analysis with metabolic models. *Brief Bioinform* 2013:1–20. doi: 10.1093/bib/bbs071.
38. Locasale JW. Metabolic rewiring drives resistance to targeted cancer therapy. *Mol Syst Biol* 2012, 8:597.
39. Folger O, Jerby L, Frezza C, Gottlieb E, Rupp E. Predicting selective drug targets in cancer through metabolic networks. *Mol Syst Biol* 2011, 7:501.
40. Covert MW, Schilling CH, Palsson BØ. Regulation of gene expression in flux balance models of metabolism. *J Theor Biol* 2001, 213:73–88.
41. Herrgård MJ, Lee B-S, Portnoy V, Palsson BØ. Integrated analysis of regulatory and metabolic networks reveals novel regulatory mechanisms in *Saccharomyces cerevisiae*. *Genome Res* 2006, 16:627–635.
42. Dingel J, Milenkovic O. List-decoding methods for inferring polynomials in finite dynamical gene network models. *Bioinformatics* 2009, 25:1686–1693.
43. Dimitrova E, Garcia-Puente LD, Hinkelmann F, Jarrah AS, Laubenbacher R, Stigler B, Stillman M, Vera-Licona P. Parameter estimation for Boolean models of biological networks. *Theor Comput Sci* 2011, 412:2816–2826.
44. Stigler B, Jarrah A, Stillman M, Laubenbacher R. Reverse engineering of dynamic networks. *Ann N Y Acad Sci* 2007, 1115:168–177.
45. Jarrah AS, Laubenbacher R, Stigler B, Stillman M. Reverse-engineering of polynomial dynamical systems. *Adv Appl Math* 2007, 39:477–489.
46. Shlomi T, Berkman O, Rupp E. Regulatory on/off minimization of metabolic flux. *Proc Natl Acad Sci U S A* 2005, 102:7695–7700.
47. Segrè D, Vitkup D, Church GM. Analysis of optimality in natural and perturbed metabolic networks. *Proc Natl Acad Sci U S A* 2002, 99:15112–15117.
48. Lee D, Chandrasekaran S, Price ND. Improving metabolic flux predictions using absolute gene expression data. *BMC Syst Biol* 2012, 6:73.
49. Chandrasekaran S, Price ND. Probabilistic integrative modeling of genome-scale metabolic and regulatory

- networks in *Escherichia coli* and *Mycobacterium tuberculosis*. *Proc Natl Acad Sci U S A* 2010, 107:17845–17850.
50. Imielinski M, Belta C. Deep epistasis in human metabolism. *Chaos* 2010, 20:026104.
51. Imielinski M, Belta C. Exploiting the pathway structure of metabolism to reveal high-order epistasis. *BMC Syst Biol* 2008, 2:40.
52. Xu L, Barker B, Gu Z. Dynamic epistasis for different alleles of the same gene. *Proc Natl Acad Sci U S A* 2012, 109:10420–10425. doi: 10.1073/pnas.1121507109.
53. He X, Qian W, Wang Z, Li Y, Zhang J. Prevalent positive epistasis in *Escherichia coli* and *Saccharomyces cerevisiae* metabolic networks. *Nat Genet* 2010, 42:272–276.
54. Resendis-Antonio O, Checa A, Encarnación S. Modeling core metabolism in cancer cells: surveying the topology underlying the Warburg effect. *PLoS One* 2010, 5:e12383.
55. Shlomi T, Benyamini T, Gottlieb E, Sharan R, Ruppin E. Genome-scale metabolic modeling elucidates the role of proliferative adaptation in causing the Warburg effect. *PLoS Comput Biol* 2011, 7:e1002018.
56. Vazquez A, Oltvai ZN. Molecular crowding defines a common origin for the Warburg effect in proliferating cells and the lactate threshold in muscle physiology. *PLoS One* 2011, 6:e19538.
57. Frezza C, Zheng L, Folger O, Rajagopalan KN, MacKenzie ED. Haem oxygenase is synthetically lethal with the tumour suppressor fumarate hydratase. *Nature* 2011, 477:225–228.
58. Thiele I, Swainston N, Fleming RMT, Hoppe A, Sahoo S. A community-driven global reconstruction of human metabolism. *Nat Biotechnol* 2013, 31:1–9. doi: 10.1038/nbt.2488.
59. Gianchandani EP, Chavali AK, Papin JA. The application of flux balance analysis in systems biology. *Wiley Interdiscip Rev Syst Biol Med* 2009, 2:372–382.
60. Lewis NE, Nagarajan H, Palsson BØ. Constraining the metabolic genotype-phenotype relationship using a phylogeny of in silico methods. *Nat Rev Microbiol* 2012, 10:291–305.
61. Sangar V, Eddy JA, Simeonidis E, Price ND. Mechanistic modeling of aberrant energy metabolism in human disease. *Front Physiol* 2012, 3:404.
62. Lerman JA, Hyduke DR, Latif H, Portnoy VA, Lewis E. In silico method for modelling metabolism and gene product expression at genome scale. *Nat Commun* 2012, 3:929.
63. Karr JRSanghvi JC, Macklin DN, Gutschow MV, Jacobs JM. A whole-cell computational model predicts phenotype from genotype. *Cell* 2012, 150:389–401.
64. Yizhak K, Benyamini T, Liebermeister W, Ruppin E, Shlomi T. Integrating quantitative proteomics and metabolomics with a genome-scale metabolic network model. *Bioinformatics* 2010, 26:i255–i260.
65. Herrgård MJ, Swainston N, Dobson P, Dunn WB, Arga KY. A consensus yeast metabolic network reconstruction obtained from a community approach to systems biology. *Nat Biotechnol* 2008, 26:1155–1160.
66. Karr JR, Sanghvi JC, Macklin DN, Arora A, Covert MW. WholeCellKB: model organism databases for comprehensive whole-cell models. *Nucleic Acids Res* 2013, 41:D787–D792.
67. <http://kbase.science.energy.gov/> (Accessed March 3, 2013).
68. Pabinger S, Rader R, Agren R, Nielsen J, Trajanoski Z. MEMOSys: bioinformatics platform for genome-scale metabolic models. *BMC Syst Biol* 2011, 5:20.
69. Helikar T, Kowal B, McClenathan S, Bruckner M, Rowley T, Madrahimov A. The cell collective: toward an open and collaborative approach to systems biology. *BMC Syst Biol* 2012, 6:96.
70. Heinrich R, Schuster S. *The Regulation of Cellular Systems*. New York: Springer; 1996.
71. Van Riel NAW. Dynamic modelling and analysis of biochemical networks: mechanism-based models and model-based experiments. *Brief Bioinform* 2006, 7:364–374.
72. Beard DA. Simulation of cellular biochemical system kinetics. *Wiley Interdiscip Rev Syst Biol Med* 2012, 3:136–146.
73. Cornish-Bowden A. *Fundamentals of Enzyme Kinetics*. 4th Edition. Weinheim, Germany: Wiley-Blackwell; 2012:498.
74. Segel IH. *Enzyme Kinetics. Behavior and Analysis of Rapid Equilibrium and Steady-State Enzyme System*. New York: John Wiley & Sons, Inc.; 1993.
75. Dash RK, Li Y, Kim J, Beard DA, Saidel GM, Cabrera ME. Metabolic dynamics in skeletal muscle during acute reduction in blood flow and oxygen supply to mitochondria: in-silico studies using a multi-scale, top-down integrated model. *PLoS One* 2008, 3:e3168.
76. Dash RK, Li Y, Kim J, Saidel GM, Cabrera ME. Modeling cellular metabolism and energetics in skeletal muscle: large-scale parameter estimation and sensitivity analysis. *IEEE Trans Bio-Med Eng* 2008, 55:1298–1318.
77. Costa RS, Machado D, Rocha I, Ferreira EC. Hybrid dynamic modeling of *Escherichia coli* central metabolic network combining Michaelis-Menten and approximate kinetic equations. *Biosystems* 2010, 100:150–157.
78. Bulik S, Grimbs S, Huthmacher C, Selbig J, Holzhütter HG. Kinetic hybrid models composed of mechanistic and simplified enzymatic rate laws—a promising method for speeding up the kinetic

- modelling of complex metabolic networks. *FEBS J* 2009, 276:410–424.
79. Schomburg I, Chang A, Placzek S, Söhngen C, Rother M, Lang M, Munaretto C, Ulas S, Stelzer M, Grote A, Scheer M, Schomburg D. BRENDA in 2013: integrated reactions, kinetic data, enzyme function data, improved disease classification: new options and contents in BRENDA. *Nucleic Acids Res* 2013, 41:D764–D772.
 80. Wittig U, Kania R, Kania R, Golebiewski M, Rey M, Shi L, Jong L, Alga E, Weidemann A, Sauer-Danzwith H, Mir S, et al. SABIO-RK-database for biochemical reaction kinetics. *Nucleic Acids Res* 2012.
 81. Goldberg RN, Tewari YB, Bhat TN. Thermodynamics of enzyme-catalyzed reactions—a database for quantitative biochemistry. *Bioinformatics* 2004, 20:2874–2877.
 82. McDonald AG, Boyce S, Tipton KF. ExplorEnz: the primary source of the IUBMB enzyme list. *Nucleic Acids Res* 2009, 37:D593–D597.
 83. Caspi R, Altman T, Dreher K, Fulcher CA, Subhraveti P, Keseler IM, Kothari A, Krummenacker M, Latendresse M, Mueller LA et al. The MetaCyc database of metabolic pathways and enzymes and the BioCyc collection of pathway/genome databases. *Nucleic Acids Res* 2012, 40:D742–D753.
 84. Wishart DS, Knox C, Guo AC, Eisner R, Young N, Gautam B, Hau DD, Psychogios N, Dong E, Bouatra S. HMDB: a knowledgebase for the human metabolome. *Nucleic Acids Res* 2009, 37(Database issue):D603–D610.
 85. Mendes P. Biochemistry by numbers: simulation of biochemical pathways with Gepasi 3. *Trends Biochem Sci* 1997, 22:361–363.
 86. Vanlier J, Wu F, Qi F, Vinnakota KC, Han Y, Dash RK, Yang F, Beard DA. BISEN: biochemical simulation environment. *Bioinformatics* 2009, 25:836–837.
 87. Hofmeyr JH, Westerhoff HV. Building the cellular puzzle: control in multi-level reaction networks. *J Theor Biol* 2001, 208:261–285.
 88. Aubert A, Costalat R. Interaction between astrocytes and neurons studied using a mathematical model of compartmentalized energy metabolism. *J Cereb Blood Flow Metab* 2005, 25:1476–1490.
 89. Cloutier M, Bolger FB, Lowry JP, Wellstead P. An integrative dynamic model of brain energy metabolism using in vivo neurochemical measurements. *J Comput Neurosci* 2009, 27:391–414.
 90. DiNuzzo M, Mangia S, Maraviglia B, Giove F. Changes in glucose uptake rather than lactate shuttle take center stage in subserving neuroenergetics: evidence from mathematical modeling. *J Cereb Blood Flow Metab* 2010, 30:586–602.
 91. Zhou L, Cabrera ME, Okere IC, Sharma N, Stanley WC. Regulation of myocardial substrate metabolism during increased energy expenditure: insights from computational studies. *Am J Physiol Heart Circ Physiol* 2006, 291:H1036–H1046.
 92. Wu F, Zhang EY, Zhang J, Bache RJ, Beard DA. Phosphate metabolite concentrations and ATP hydrolysis potential in normal and ischaemic hearts. *J Physiol* 2008, 586:4193–4208.
 93. Wellstead P, Cloutier M. An energy systems approach to Parkinson's disease. *Wiley Interdiscip Rev Syst Biol Med* 2011, 3:1–6.
 94. Van Stiphout RGPM, van Riel NAW, Verhoog PJ, Hilbers PAJ, Nicolay K, Jeneson JAL. Computational model of excitable cell indicates ATP free energy dynamics in response to calcium oscillations are undamped by cytosolic ATP buffers. *Syst Biol* 2006, 153:405–408.
 95. Zheng Y, Rundell A. Comparative study of parameter sensitivity analyses of the TCR-activated Erk-MAPK signalling pathway. *IEE Proc Syst Biol* 2006, 153:201.
 96. Kacser H, Burns JA. The control of flux. *Symp Soc Exp Biol* 1973, 27:65–104.
 97. Heinrich R, Rapoport T. A linear steady state treatment of enzymatic chains. *Eur J Biochem* 1974, 95:89–95.
 98. Hyduke D., Schellenberger J, Que R, Fleming R, Thiele I, Orth J, Feist A, Zielinski D, Bordbar A, Lewis N, et al. COBRA Toolbox 2.0. 2011. doi: 10.1038/protex.2011.234
 99. Sauer UWE, Lasko DR, Fiaux J, Glaser R, Szyperski T, Wüthrich K, Bailey JE, Hochuli M, Wu K. Metabolic flux ratio analysis of genetic and environmental modulations of *Escherichia coli* central carbon metabolism metabolic flux ratio analysis of genetic and environmental modulations of *Escherichia coli* central carbon metabolism. *J Bacteriol* 1999, 181:6679–6688.
 100. Wiechert W, Möllney M, Isermann N, Wurzel M, de Graaf AA. Bidirectional reaction steps in metabolic networks: III. Explicit solution and analysis of isotopomer labeling systems. *Biotechnol Bioeng* 1999, 66:69–85.
 101. Wiechert W, Wurzel M. Metabolic isotopomer labeling systems. Part I: global dynamic behavior. *Math Biosci* 2001, 169:173–205.
 102. Wiechert W. ¹³C metabolic flux analysis. *Metab Eng* 2001, 3:195–206.
 103. Antoniewicz MR, Kelleher JK, Stephanopoulos G. Elementary metabolite units (EMU): a novel framework for modeling isotopic distributions. *Metab Eng* 2007, 9:68–86.
 104. Shestov AA, Valette J, Deelchand DK, Uğurbil K, Henry P-G. Metabolic modeling of dynamic brain ¹³C NMR multiplet data: concepts and simulations with a two-compartment neuronal-glia model. *Neurochem Res* 2012, 37:2388–2401.

105. Yuan J, Bennett BD, Rabinowitz JD. Kinetic flux profiling for quantitation of cellular metabolic fluxes. *Nat Protoc* 2008, 3:1328–1340.
106. Van Winden WA, Heijnen JJ, Verheijen PJT. Cumulative bondomers: a new concept in flux analysis from 2D [¹³C,¹H] COSY NMR data. *Biotechnol Bioeng* 2002, 80:731–745.
107. Quek LE, Wittmann C, Nielsen L, Kromer J. OpenFLUX: efficient modelling software for ¹³C-based metabolic flux analysis. *Microb Cell Fact* 2009, 8:25.
108. Wiechert W, Möllney M, Petersen S, de Graaf AA. A universal framework for ¹³C metabolic flux analysis. *Metab Eng* 2001, 3:265–283.
109. Poskar CH, Huege J, Krach C, Franke M, Shachar-Hill Y, Junker B. iMS2Flux — a high-throughput processing tool for stable isotope labeled mass spectrometric data used for metabolic flux analysis. *BMC Bioinformatics* 2012, 13:295.
110. Weitzel M, Nöh K, Dalman T, Niedenführ S, Stute B, Wiechert W. 13CFLUX2-high-performance software suite for ¹³C-metabolic flux analysis. *Bioinformatics* 2013, 29:143–145.
111. Zamboni N, Fischer E, Sauer U. FiatFlux — a software for metabolic flux analysis from ¹³C-glucose experiments. *BMC Bioinformatics* 2005, 6:209.
112. Murphy TA, Young JD. ETA: Robust software for determination of cell specific rates from extracellular time courses. *Biotechnol Bioeng* 2013, 110:1748–1758.
113. Sriram G, Fulton DB, Iyer VV, Peterson JM, Zhou R, Westgate ME, Spalding MH, Shanks JV. Quantification of Compartmented Metabolic Fluxes in Developing Soybean Embryos by Employing Biosynthetically Directed Fractional ¹³C Labeling, Two-Dimensional [¹³C, ¹H] Nuclear Magnetic Resonance, and Comprehensive Isotopomer Balancing 1 [w]. *Plant Physiol* 2004, 136:3043–3057.
114. Mason GF, Falk Petersen K, de Graaf RA, Kanamatsu T, Otsuki T, Shulman GI, Rothman DL. A comparison of (¹³C)NMR measurements of the rates of glutamine synthesis and the tricarboxylic acid cycle during oral and intravenous administration of [1-(¹³C)]glucose. *Brain Res Brain Res Protoc* 2003, 10:181–190.
115. Svijsovic M, Olivares-Hernández R, Agren R, Dahr N, Vongsangnak W, Nookaew I, Patil KR, Nielsen J. BioMet Toolbox: genome-wide analysis of metabolism. *Nucleic Acids Res* 2010, 38:W149.
116. Henry P-G, Adriany G, Deelchand D, Gruetter R, Marjanska M, Oz G, Seaquist ER, Shestov A, Ugurbil K. In vivo ¹³C NMR spectroscopy and metabolic modeling in the brain: a practical perspective. *Magn Reson Imaging* 2006, 24:527–539.
117. Henry P, Henry PG, Deelchand DK, Iltis I, Marjanska M, Öz G, Shestov A, Valette J. *Neural Metabolism In Vivo*, vol. 4. Boston, MA: Springer; 2012, 181–220.
118. Mason GF, Rothman DL. Basic principles of metabolic modeling of NMR (¹³C) isotopic turnover to determine rates of brain metabolism in vivo. *Metab Eng* 2004, 6:75–84.
119. Rothman DL, De Feyter HM, De Graaf RA, Mason GF, Behar KL. ¹³C MRS studies of neuroenergetics and neurotransmitter cycling in humans. *NMR Biomed* 2011, 24:943–957.
120. Zamboni N. ¹³C metabolic flux analysis in complex systems. *Curr Opin Biotechnol* 2011, 22:103–108.
121. Sauer U. Metabolic networks in motion: ¹³C-based flux analysis. *Mol Syst Biol* 2006, 2:62.
122. Shachar-Hill Y. Metabolic network flux analysis for engineering plant systems. *Curr Opin Biotechnol* 2013, 24:1–9. doi: 10.1016/j.copbio.2013.01.004.
123. Antoniewicz MR, Kelleher JK, Stephanopoulos G. Determination of confidence intervals of metabolic fluxes estimated from stable isotope measurements. *Metab Eng* 2006, 8:324–337.
124. Du F, Zhu X-H, Zhang Y, Friedman M, Zhang N, Ugurbil K, Chen W. Tightly coupled brain activity and cerebral ATP metabolic rate. *Proc Natl Acad Sci U S A* 2008, 105:6409–6414.
125. Zhu X-H, Du F, Zhang N, Zhang Y, Lei H, Qiao H, Ugurbil K, Chen W. Multi-Modal Methods and In Vivo Applications. In: Hyder F, ed. *Dynamic Brain Imaging*, vol. 489. Humana Press; 2009, 317–357.
126. Zhu X-H, Zhang N, Zhang Y, Ugurbil K, Chen W. New insights into central roles of cerebral oxygen metabolism in the resting and stimulus-evoked brain. *J Cereb Blood Flow Metab* 2009, 29:10–18.
127. Bederman IR, Dufner DA, Alexander JC, Previs SF. Novel application of the “doubly labeled” water method: measuring CO₂ production and the tissue-specific dynamics of lipid and protein in vivo. *Am J Physiol Endocrinol Metab* 2006, 290:E1048–E1056.
128. Rodrigues TB, Cerdán S. A fast and sensitive ¹H NMR method to measure the turnover of the H₂ hydrogen of lactate. *Magn Reson Med* 2005, 54:1014–1019.
129. Ugurbil K, Rottenberg H, Glynn P, Shulman RG. ³¹P nuclear magnetic resonance studies of bioenergetics and glycolysis in anaerobic *Escherichia coli* cells. *Proc Natl Acad Sci U S A* 1978, 75:2244–2248.
130. Eakin RT, Morgan LO, Gregg CT, Matwiyoff NA. Carbon-13 nuclear magnetic resonance spectroscopy of living cells and their metabolism of a specifically labeled ¹³C substrate. *FEBS Lett* 1972, 28:259–264.
131. Ugurbil K, Brown TR, Den Hollander JA, Glynn P, Shulman RG. High-resolution ¹³C nuclear magnetic resonance studies of glucose metabolism in *Escherichia coli*. *Proc Natl Acad Sci U S A* 1978, 75: 3742–3746.
132. Chance EM, Seeholzer SH, Kobayashi K, Williamson JR. Mathematical analysis of isotope labeling in the citric acid cycle with applications to ¹³C NMR

- studies in perfused rat hearts. *J Biol Chem* 1983, 258:13785–13794.
133. Malloy CR, Sherry AD, Jeffrey FM. Evaluation of carbon flux and substrate selection through alternate pathways involving the citric acid cycle of the heart by ^{13}C NMR spectroscopy. *J Biol Chem* 1988, 263:6964–6971.
134. Cohen S. Effects of ethanol on alanine metabolism in perfused mouse liver studied by ^{13}C NMR. *Proc Natl Acad Sci U S A* 1979, 76:4808–4812.
135. Vogt JA, Yarmush DM, Yu YM, Zupke C, Fischman AJ, Tompkins RG. TCA cycle flux estimates from NMR- and GC-MS-determined [^{13}C]glutamate isotopomers in liver. *Am J Physiol* 1997, 272:C2049–C2062.
136. Di Donato L, Des Rosiers C, Montgomery JA, David F, Garneau M, Brunengraber H. Rates of gluconeogenesis and citric acid cycle in perfused livers, assessed from the mass spectrometric assay of the ^{13}C labeling pattern of glutamate. *J Biol Chem* 1993, 268:4170–4180.
137. Mason GF, Rothman DL, Behar KL, Shulman RG. NMR determination of the TCA cycle rate and alpha-ketoglutarate/glutamate exchange rate in rat brain. *J Cereb Blood Flow Metab* 1992, 12: 434–447.
138. Fitzpatrick SM, Hetherington HP, Behar KL, Shulman RG. The flux from glucose to glutamate in the rat brain in vivo as determined by ^1H -observed, ^{13}C -edited NMR spectroscopy. *J Cereb Blood Flow Metab* 1990, 10:170–179.
139. Bloch G, Chase JR, Meyer DB, Avison MJ, Shulman GI, Shulman RG. In vivo regulation of rat muscle glycogen resynthesis after intense exercise. *Am J Physiol* 1994, 266:E85–E91.
140. Szczepaniak L, Babcock EE, Malloy CR, Sherry AD. Oxidation of acetate in rabbit skeletal muscle: detection by ^{13}C NMR spectroscopy in vivo. *Magn Reson Med* 1996, 36:451–457.
141. Goodacre R, Vaidyanathan S, Dunn WB, Harrigan GG, Kell DB. Metabolomics by numbers: acquiring and understanding global metabolite data. *Trends Biotechnol* 2004, 22:245–252.
142. Gruetter R, Seaquist ER, Ugurbil K. A mathematical model of compartmentalized neurotransmitter metabolism in the human brain. *Am J Physiol Endocrinol Metab* 2001, 281:E100–E112.
143. Chen W, Zhu XH, Gruetter R, Seaquist, ER, Adriany G, Ugurbil K. Study of tricarboxylic acid cycle flux changes in human visual cortex during hemifield visual stimulation using (^1H -[^{13}C]) MRS and fMRI. *Magn Reson Med* 2001, 45:349–355.
144. Boumezbeur F, Mason GF, de Graaf RA, Behar KL, Cline GW, Shulman GI, Rothman DL, Petersen KF. Altered brain mitochondrial metabolism in healthy aging as assessed by in vivo magnetic resonance spectroscopy. *J Cereb Blood Flow Metab* 2010, 30:211–221.
145. Choi J, Grossbach MT, Antoniewicz MR. Measuring complete isotopomer distribution of aspartate using gas chromatography/tandem mass spectrometry. *Anal Chem* 2012, 84:4628–4632.
146. Lanz B, Uffmann K, Wyss MT, Weber B, Buck A, Gruetter R. A two-compartment mathematical model of neuroglial metabolism using [$1-(^{11}\text{C})$] acetate. *J Cereb Blood Flow Metab* 2012, 32:548–559.